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#### **Technical Section**

## Exploration of blood flow patterns in cerebral aneurysms during the cardiac cycle<sup>\*</sup>

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#### ABSTRACT

This paper presents a method for clustering time-dependent blood flow data, represented by path lines, in cerebral aneurysms using a reliable similarity measure combined with a clustering technique. Such aneurysms bear the risk of rupture, whereas their treatment also carries considerable risks for the patient. Medical researchers emphasize the importance of investigating aberrant blood flow patterns for the patient-specific rupture risk assessment and treatment analysis. Therefore, occurring flow patterns are manually extracted and classified according to predefined criteria. The manual extraction is time-consuming for larger studies and affected by visual clutter, which complicates the subsequent classification of flow patterns. In contrast, our method allows an automatic and reliable clustering of intra-aneurysmal flow patterns that facilitates their classification. We introduce a similarity measure that groups spatio-temporally adjacent flow patterns. We combine our similarity measure with a commonly used clustering technique and applied it to five representative datasets. The clustering results are presented by 2D and 3D visualizations and were qualitatively compared and evaluated by four domain experts. Moreover, we qualitatively evaluated our similarity measure.

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#### 1 1. Introduction

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For the diagnosis and treatment assessment of cardiovascular 2 3 diseases (CVDs), the analysis of patient-specific morphological and hemodynamic data is necessary [1]. This work focuses on cerebral 4 aneurysms, characterizing pathologic dilatations of intracranial ar-5 teries. Their most serious consequence is their rupture leading to 6 a subarachnoid hemorrhage (SAH), which is associated with a high 7 mortality and morbidity rate [2]. In case of a rupture, a treatment 8 is essential. A frequently used treatment option is stenting, where 9 the flow is diverted from the aneurysm sac by an expandable med-10 ical implant (stent). However, treatment is also associated with a 11 12 considerable risk of severe complications, such as post-treatment 13 hemorrhaging, which can exceed the natural rupture risk [3]. In most cases an aneurysm is asymptomatic and will never rupture. 14 But due to the poor prognosis of a SAH, aneurysms are usually 15 treated. Thus, it is highly desirable to better understand the indi-16 vidual rupture risk and to restrict treatment to high-risk patients. 17

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Unfortunately, the aneurysm progression and rupture depends 18 on different factors such as genetics, morphological conditions and 19 hemodynamics, where their interplay is not well understood [4]. 20 Hemodynamic data are characterized by quantitative parameters 21 such as Wall Shear Stress (WSS), and qualitatively, e.g., w.r.t. spe-22 cific flow patterns, such as vortices. Moreover, flow patterns are 23 assumed to be related to the success of treatment and their dis-24 tance to the vessel wall seems to be an important factor for the 25 assessment of the aneurysm's state [5]. 26

To investigate the influence of flow patterns on the aneurysm's 27 rupture, medical studies are performed [6]. Therefore, hemody-28 namic information are used that can be obtained by Computational 29 Fluid Dynamic (CFD) simulations. Flow patterns are extracted and 30 manually classified according to their complexity and stability dur-31 ing the cardiac cycle. The results were compared between ruptured 32 and non-ruptured cases to identify characteristics associated with 33 rupture. This is a time-consuming process in which flow patterns 34 more distant to the wall are easily overlooked due to visual clut-35 ter and occlusion. To uncover correlations between flow patterns 36 and the aneurysm state, more efficient analysis techniques are es-37 sential. This requires a reliable grouping of blood flow-representing 38 path lines characterizing individual flow patterns. 39

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40 In this work, we present a method for an automatic clustering 41 of blood flow in cerebral aneurysms over the cardiac cycle. Blood 42 flow-representing path lines were integrated in simulated CFD data 43 and clustered to obtain groups with similar flow behavior. For this purpose, we extend an established similarity measure for stream-44 lines to path lines that incorporates their temporal component. To 45 explore the behavior of individual flow patterns, we provide 2D 46 views linked to a 3D depiction of the aneurysm wall and inter-47 48 nal blood flow. The 2D views enable an occlusion-free visualization of flow patterns, including their distance to the vessel wall. The 49 50 3D visualization represents the focus upon which the exploration 51 of morphological aneurysm characteristics together with the blood flow information over the cardiac cycle takes place. We integrate 52 53 these techniques into a framework that we developed in collaboration with domain experts. In summary, we make the following 54 contributions: 55

- An automatic clustering of intra-aneurysmal flow patterns over the cardiac cycle.
- A linked 2D and 3D view of the aneurysm surface and internal flow patterns for an interactive exploration.

#### 60 2. Related work

61 Our work is related to partition-based blood flow visualization, 62 as well as the visual exploration of aneurysm data.

#### 63 2.1. Partition-based flow visualization

Partitioning techniques decompose flow into areas of common 64 structure to investigate hemodynamics. Graphical representatives 65 66 of flow regions can be computed to generate a visual summary or a subsequent visualization can be restricted to regions with specific 67 68 properties, e.g., vortices. Such techniques are mainly based on integral curves, since in contrast to local vectorial flow data, they rep-69 resent continuous flow patterns. The partitioning is performed in 70 a user-guided [7–9] or automatic fashion [10–14]. Less frequently, 71 72 local flow vectors [15] or aneurysm wall properties [16,17] are 73 employed.

User-guided techniques partition integral curves based on line 74 predicates (LP) [18], which are Boolean functions that decide if in-75 tegral curves fulfill properties of interest. Gasteiger et al. [8] ap-76 77 plied LP to CFD data of cerebral aneurysms to extract flow features, e.g., the inflow jet - the structure of high-speed, parallel 78 aneurysm inflow and the *impingement zone* – the region where the 79 inflow jet hits the wall with high impact. Based on this, a compar-80 81 ative visualization for evaluating various stent configurations was 82 presented, integrating morphological and hemodynamic data [19]. 83 Born et al. [7] utilized LP to identify relevant flow features such as 84 jets and vortices in measured cardiac data. Köhler et al. [9] used different local vortex criteria as LP to filter path lines that repre-85 86 sent aortic vortices.

87 Automatic techniques employ a data-driven approach and utilize clustering methods to group integral curves based on a 88 similarity measure. McLoughlin et al. [14] introduced a streamline 89 similarity measure by computing geometrical features based on 90 91 the underlying vector field and used an agglomerative hierarchical 92 clustering (AHC) with average link for partitioning. Their method 93 was applied to time-dependent data by extracting the geometrical 94 features from the vector field of the corresponding time step. However, the temporal component was not directly considered. Two 95 geometrically similar path lines occurring in non-overlapping time 96 intervals would have a high similarity. Oeltze et al. [13] compared 97 multiple streamline clusterings in the context of aneurysm hemo-98 dynamics. Streamline similarities were computed based on line ge-99 100 ometry [20]. They conducted a quantitative evaluation of k-Means, AHC, and spectral clustering (SC) w.r.t. cluster purity measures, 101 where SC as well as AHC with average link and Ward's method 102 performed best. Furthermore, a visual summary of blood flow was 103 proposed, containing one representative streamline per cluster to 104 reduce visual clutter. Englund et al. [10] employed a partitioning 105 approach for the exploration of aortic hemodynamics. They used 106 the Finite-time Lyapunov Exponent to measure the separation of 107 path lines and coherent areas are derived. Liu et al. [11] measured 108 path line similarities using an octree. The space is divided into 109 cubes either by equidistant length or by adaptive length that 110 depends on the features of the underlying vector field. A sequence 111 is assigned to the path lines that incorporates the passed cubes, 112 where the similarity is based on the longest common sequence. 113 Meuschke et al. [12] compared multiple clustering methods of 114 path lines representing aortic vortex flow. Path line similarities 115 were computed based on the spatio-temporal coordinates of line 116 endpoints and the line's average distance to the vessel centerline. 117 AHC with average link performed best in separating vortices. 118

We introduce a time-dependent clustering of flow-representing 119 path lines by extending an eligible approach for streamline clus-120 tering [20]. In contrast to the streamline similarity measure by 121 McLoughlin et al. [14], our method directly incorporates the tem-122 poral component. If a flow pattern occurs, decays and reoccurs dur-123 ing the cardiac cycle, our method results in several clusters. This is 124 required, since stability of flow patterns is an important criterion 125 in medical studies to predict the rupture risk [6]. Existing meth-126 ods are not able to represent instable flow patterns by different 127 clusters. Moreover, compared to existing time-dependent cluster-128 ing approaches [11,12], we are not dependent on the centerline or 129 the underlying partitioning of the space. 130

#### 2.2. Visualization and exploration of aneurysms

To visualize the aneurysm morphology, Hastreiter 132 et al. [21] presented a direct volume rendering (DVR) method. 133 Tomandl et al. [22] introduced a standardized vessel depiction 134 using DVR for a more objective assessment of the aneurysm 135 morphology. 136

Several works parametrize the aneurysm surface to generate 137 more abstract representations. Goubergrits et al. [23] mapped the 138 aneurysm to a uniform sphere to analyze statistical WSS distribu-139 tions. Meuschke et al. [24] generated a 2D aneurysm map by using 140 least squares conformal maps [25] that provides an occlusion-free 141 overview visualization. Tao et al. [26] presented the VesselMap, a 142 2D mapping of an aneurysm and parent vasculature formulated as 143 a graph layout optimization problem. 144

For the simultaneous exploration of anatomical and vectorial 145 flow data, Gasteiger et al. [27] introduced the FlowLens, an in-146 teractive focus-and-context approach. However, outside the lens 147 area, the flow cannot be observed. To improve this, Lawonn 148 et al. [28] provided a vessel visualization such that the morphology 149 can be better perceived and the flow is always visible. For a more 150 detailed analysis, Neugebauer et al. [17] developed a qualitative ex-151 ploration of near-wall hemodynamics in cerebral aneurysms. Sev-152 eral 2D widgets are used to simplify streamlines at different sur-153 face positions. Gambaruto et al. [29] analyzed flow features that 154 are potentially related to aneurysm rupture. They extracted criti-155 cal points related to WSS, vortices and surface shear lines, which 156 are visualized using standard techniques such as glyphs, vortex-157 isosurfaces, and streamlines. Lawonn et al. [30] presented a frame-158 work for an occlusion-free blood flow visualization by using illus-159 trative techniques. Meuschke et al. [24] extended this approach to 160 investigate morphological and hemodynamic data simultaneously 161 by providing a low-occlusion 2.5D view linked to a 3D aneurysm 162 depiction. 163

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